

Rapid Neuromodulatory Actions of Integrin Ligands

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Extracellular matrix (ECM) proteins and their receptors, the integrins, actively participate in the control of many fundamental cellular functions in the developing nervous system, including the regulation of cell migration, differentiation, and survival and the control of neurite outgrowth. ECM–integrin interactions in the mature nervous system are commonly considered to be more static in nature and of little importance in the regulation of neuronal function. In contrast, we demonstrate that integrins and their ligands are capable of rapid neuromodulatory actions. Specifically, we show that integrin ligands can alter neuronal

pacemaker properties, intracellular free Ca^{2+} levels, and voltage-gated Ca^{2+} currents in a matter of minutes. These findings indicate that ECM–integrin interactions play a dynamic role in regulating the physiological status of mature neurons, a process that may contribute to synaptic plasticity, neural regeneration, and neuropathology.

Key words: ECM; extracellular matrix proteins; fibronectin; RGD; integrins; Ca^{2+} signaling; voltage-gated Ca^{2+} currents; pacemaker properties; neuron; cell adhesion; mollusks

Integrins, a family of evolutionarily conserved heterodimeric transmembrane proteins, are the main cell-surface receptors for extracellular matrix (ECM) proteins such as fibronectin (FN), laminin, and collagen (Aplin et al., 1998; Burke, 1999; Giancotti and Ruoslahti, 1999; Hughes, 2001). Like many other cell adhesion receptors, integrins serve a dual purpose in that they participate in both cell adhesion and transmembrane signal transduction. In the latter role, they may trigger a variety of cellular responses ranging from the activation of cytosolic phospholipases and kinases to changes in intracellular free Ca^{2+} concentration ($[\text{Ca}^{2+}]_i$) (Sjaastad and Nelson, 1997; Aplin et al., 1998). In both their adhesive and signaling capacity, integrins play a vital role in morphogenesis and maintenance of most animal tissues, including the nervous system (Reichardt and Tomaselli, 1991; Venstrom and Reichardt, 1993; Giancotti and Ruoslahti, 1999; De Arcangelis and Georges-Labouesse, 2000; Perris and Perissinotto, 2000; Tarone et al., 2000).

Although numerous studies emphasize the versatile and dynamic nature of integrin–ECM interactions in the development of the nervous system, knowledge of integrin function in the adult nervous system has been slower to arrive. Recent indications are that integrin–ECM interactions play a much more dynamic role in the adult nervous system than previously thought. For example, they are increasingly implicated in synaptic plasticity and memory formation, neural regeneration, and epileptogenesis (Jones and Grooms, 1997; Grotewiel et al., 1998; Pinkstaff et al., 1998; Stäubli et al., 1998; Murase and Schuman, 1999; Benson et al., 2000; Condic, 2001). Little or nothing is known about the molecular mechanisms underlying these actions of integrins. Therefore, we explored the potential of integrin ligands for short-term neu-

romodulatory actions using a combination of electrophysiological and imaging techniques.

Our results show that integrin ligand binding can cause rapid changes in spontaneous electrical activity, $[\text{Ca}^{2+}]_i$, and high-voltage-activated (HVA) Ca^{2+} currents in mature neurons *in vitro*, thus substantiating the emerging notion that integrins and their ligands are dynamic modulators of neuronal function in the adult nervous system.

MATERIALS AND METHODS

Animals and cell isolation. Adult specimens of *Lymnaea stagnalis* (4–6 months of age; shell lengths, 25–35 mm), were taken from laboratory-raised populations. Anesthesia, aseptic dissection of the CNS, and isolation of right parietal A group (RPA) neurons were performed according to methods described previously (Wildering et al., 1995, 1998). The cells were plated in standard saline on poly-L-lysine-coated coverslips (for imaging) or poly-L-lysine-coated polystyrene culture dishes (for electrophysiological recording). All experiments were performed on cell bodies that had fully retracted their axon stumps and had not yet formed new processes.

Intracellular recording. The electrical activity of RPA neurons *in vitro* was recorded using standard high-impedance intracellular-recording techniques. Borosilicate glass electrodes were filled with a 0.5 M potassium acetate/0.05 M potassium chloride saline (impedance, >50 M Ω). The recording chamber was continuously perfused at a rate of 300–500 $\mu\text{l}/\text{min}$ with standard extracellular saline [for composition of extracellular saline, see Hermann et al. (1997)]. Peptides were applied to the saline without interrupting the flow. Before an experiment was allowed to proceed, the stability of each recording was affirmed by monitoring the resting membrane potential for at least 10 min after impaling the cell. Membrane voltages were filtered at 1 kHz and sampled at 3 kHz using Axotape 2.0.2 software (Axon Instruments, Burlingame, CA) and a Labmaster TL-1 data acquisition system (Axon Instruments).

Whole cell voltage clamp. Whole-cell Ca^{2+} currents were recorded using standard tight-seal voltage-clamp techniques. Pharmacological isolation of HVA Ca^{2+} currents was obtained by methods described previously (Wildering et al., 1995). Voltage command generation and data acquisition were achieved by means of a Labmaster TL-1 data acquisition system controlled by the pClamp 5.1 software suite (Axon Instruments). Sampled currents were corrected online for leakage current and charging transients by means of a P/3 leak subtraction protocol.

$[\text{Ca}^{2+}]_i$ imaging. $[\text{Ca}^{2+}]_i$ dynamics were imaged using conventional fura-2 AM ratiometric fluorescence techniques on isolated cells loaded with fura-2 AM-ester (15–20 min; 5 $\mu\text{g}/\text{ml}$ in 0.01% DMSO) (Molecular

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Probes, Eugene, OR). To guarantee complete hydrolysis of the probe, the cells were allowed to rest for 40–60 min after completion of fura-2 AM loading before an experiment was begun. Fluorescent image pairs (340 nm/380 nm) were acquired with an intensified CCD camera (Stanford Photonics XR-GENIII+ Ultra-blue; Solamere Technology Group, Salt Lake City, UT) coupled to an inverted microscope (Axiovert 100 TV; Zeiss, Oberkochen, Germany) and interfaced with a computer through an eight bit frame grabber board (DT3155; DataTranslation, Marlboro, MA). Illumination control, data acquisition, and data analysis were done with Axon Imaging workbench version 2.1 (build 98–109; Axon Instruments, Foster City, CA). Acquisition intervals varied from 1 to 2 min during wash periods to 2 sec during high-potassium stimulation. Raw images were corrected for background fluorescence before analysis. Data-acquisition parameters were set to obtain optimal responses in regions of interest immediately inside the plasma membrane (see Fig. 2*A*, *white ellipse*). This usually resulted in saturation of the signal in the optically thicker parts of the cell, such as the nucleus (see Fig. 2*A*, *blue sphere* in the center of the cell). The data are expressed as background-corrected 340 nm/380 nm fluorescence ratios (F_{340}/F_{380}).

Peptides and peptide application. Arg-Gly-Asp (RGD) and cyclo-Gly-Arg-Gly-Asp-Ser-Pro-Ala (cGRGDSPA) were obtained from Bachem (Torrance, CA); Gly-Arg-Gly-Asp-Ser (GRGDS) and Ser-Asp-Gly-Arg-Gly (SDGRG) were obtained from Sigma (St. Louis, MO). Human plasma FN was obtained from Boehringer Mannheim (Indianapolis, IN). In all three assays, the recording chambers were continuously perfused, and the peptides were added to the appropriate media without interrupting the flow.

Data evaluation. The variation in responsiveness between cells and the intrinsically noisy nature of most of the data necessitated an individual approach to evaluate treatment effects. We therefore adopted the following procedures. With respect to the fura-2 AM and Ca^{2+} current data, an effect was considered significant when control and treatment values measured in the same cell differed by more than two times its root mean square (RMS) amplitude. RMS amplitude, which is equivalent to the SD of the signal, control, and treatment means were calculated from 20 data points sampled under each condition. A similar procedure was used in evaluating the spike-train data. In this case, we compared action-potential intervals sampled 2 min before peptide application with intervals sampled over a similar duration at the end of the period of peptide application.

Occasionally, we used conventional parametric statistics [repeated-measures ANOVA combined with Tukey's honestly significant difference (HSD) pairwise comparison] to evaluate treatment effects within subjects. *F* statistics (ratio of mean squares of test over error mean squares) are given with corresponding degrees of freedom in their subscripts (i.e., $F_{df-test, df-error}$).

RESULTS

In this study, we used motoneurons (RPA neurons) isolated from the CNS of the pond snail *L. stagnalis*. We have shown previously that these neurons are capable of binding different ECM proteins, including FN, the latter involving an integrin-dependent adhesion mechanism (Wildering et al., 1998).

Here, we examined the effects of FN on the spontaneous electrical activity of isolated RPA neurons *in vitro*. The electrical activity of the cells was recorded 3–8 hr after plating using standard intracellular recording techniques. Under control conditions, RPA neurons are either electrically quiescent or spontaneously fire action potentials at a low rate (Fig. 1*A*). Addition of human plasma FN (1 mg/ml) to the bath significantly enhanced action-potential activity in 6 of 14 cells tested. In some cases, the effect of the protein was quite dramatic, inducing action potentials in previously quiescent cells (Fig. 1*A1*). In other cases, when cells were firing action potentials at a low rate under control conditions, FN caused a substantial increase in the firing rate (Fig. 1*A2*). The effects of FN were reversible, although complete reversal usually required more than a 30 min washing with control saline.

FN is a large multidomain protein that can interact with cells through integrin-dependent as well as integrin-independent ad-

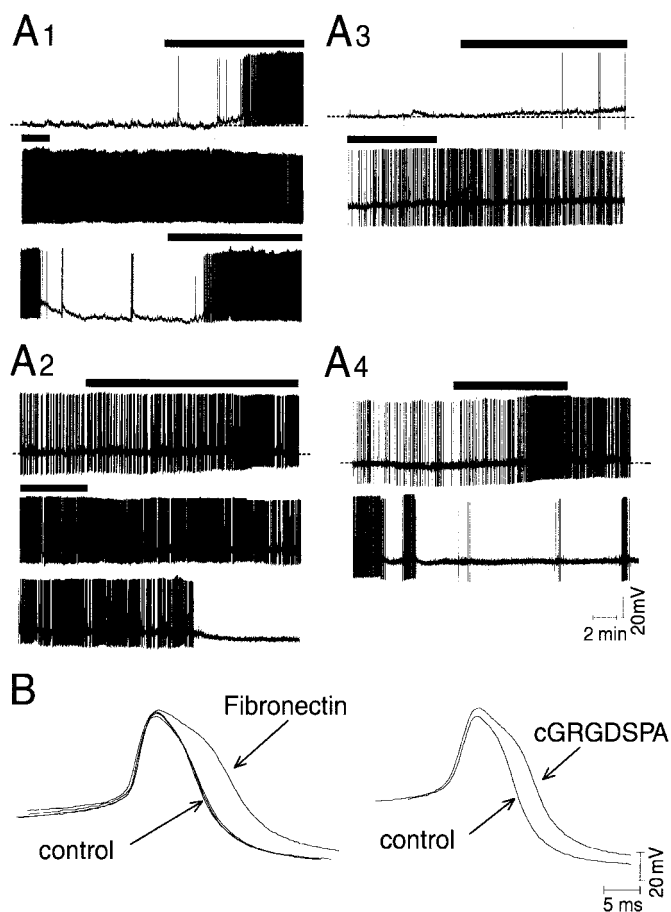


Figure 1. Effects of FN and the RGD peptide cGRGDSPA on spontaneous action-potential activity in RPA neurons *in vitro*. *A*, Membrane potential of isolated RPA neurons recorded intracellularly in control saline or saline supplemented with FN (1 μ g/ml; *A1*, *A2*, black bar above traces) or cGRGDSPA (1 μ M; *A3*, *A4*, black bar above traces). Under control conditions, isolated RPA neurons are usually electrically quiescent (*A1*, *A3*) but occasionally fire spontaneous action potentials at a low frequency (*A2*, *A4*). Introduction of FN in the bath induced spontaneous action-potential activity in previously quiescent cells (*A1*) or caused acceleration of action-potential firing in previously active cells (*A2*). The effects of FN on the action-potential activity of RPA neurons could be mimicked with cGRGDSPA, a synthetic analog of the main integrin binding site of FN (*A3*, *A4*). *B*, Treatment with FN or cGRGDSPA enhanced the duration of RPA neuron action potentials and invoked a prominent inflection in the course of the repolarization of the action potential (e.g., a Ca^{2+} shoulder).

hesion mechanisms (Potts and Campbell, 1996). Moreover, because of its large size (molecular mass of ~220 kDa), nonspecific effects on electrical activity associated with electrostatic interactions between the protein and the cells cannot be completely excluded, even at lower concentrations. Therefore, we also tested the effect of small synthetic analogs of the main integrin-binding sequence of FN (i.e., RGD peptides) (Ruoslahti, 1996). These peptides are widely used as specific integrin ligands in a variety of applications and preparations (Ruoslahti, 1996; Wu et al., 1998; Gomez et al., 2001). We previously used these peptides to confirm the involvement of integrins in FN binding by RPA neurons (Wildering et al., 1998).

We chose to use cGRGDSPA, a potent circularized RGD peptide (IC_{50} = ~110 nM in cell-adhesion assay) (Wildering et al., 1998). Figure 1*A3*, *A4* illustrates that cGRGDSPA mimics the

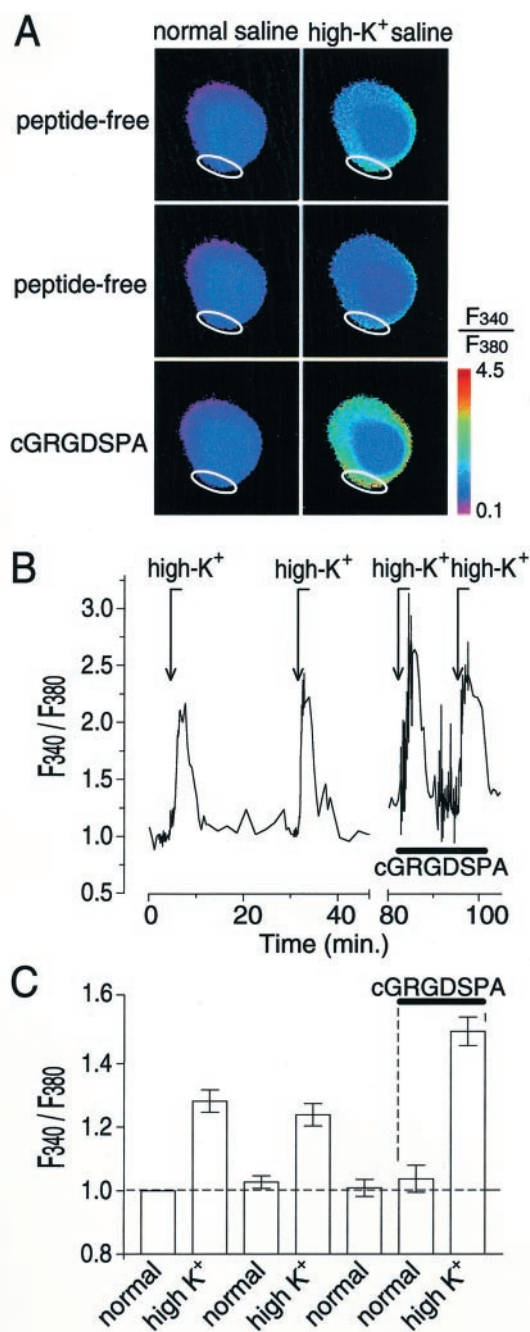


Figure 2. Effect of the RGD peptide cGRGDSPA on $[Ca^{2+}]_i$ in the cell body of RPA neurons *in vitro* as measured by fura-2 AM imaging techniques. **A**, False-color image showing fura-2 AM F_{340}/F_{380} emission intensities in the cell body of an isolated RPA neuron in normal saline (left column) and high-potassium saline (high-K⁺ saline; right column) before (top two rows labeled peptide-free) and during treatment with 1 μ M cGRGDSPA (third row labeled cGRGDSPA). Image acquisition was optimized to capture changes in the periphery of the cell (region of interest indicated by a white ellipse). As a result, the signal emanating from the nuclear area, shown as the dark blue circle in the center of the cell, was saturated (i.e., $F_{340}/F_{380} = 1$). Note that depolarization of the cell with high-K⁺ saline caused a mild increase in $[Ca^{2+}]_i$ over most of the surface area of the cell and that a second stimulation with high-K⁺ saline 30 min after the first one did not potentiate the $[Ca^{2+}]_i$ response (compare rows one and two). The $[Ca^{2+}]_i$ response induced by high-K⁺ stimulation \approx 5 min after cGRGDSPA was applied, however, was markedly enhanced in the same cell (compare rows two and three). **B**, Normalized F_{340}/F_{380} intensity measured in a cell during stimulation with high-K⁺ saline (arrows marked high-K⁺) and treatment with cGRGDSPA (indicated by

effects of FN on the spontaneous action-potential activity of RPA neurons. Superfusion of 1 μ M peptide induced action-potential activity in previously quiescent cells (Fig. 1A3) or enhanced action-potential frequency in previously active cells (Fig. 1A4). Treatment with cGRGDSPA significantly enhanced action-potential firing rates in 44% of the cells ($n = 9$). No effect on action-potential firing rates was found in the other 56% of the cells.

FN and cGRGDSPA also induced changes in the action-potential waveform (Fig. 1B). Action-potential duration increased significantly in the presence of the peptides ($F_{(9,36)} = 133.90$, $p < 0.001$; $F_{(13,57)} = 21.1$, $p < 0.001$, respectively). The increase in action-potential duration was characterized by enhancement of a shoulder in the repolarization phase of the action potential, an effect most likely involving an increase in Ca^{2+} influx through voltage-gated Ca^{2+} channels (Hermann et al., 1997). Thus, we tested the effects of RGD peptides on depolarization-dependent $[Ca^{2+}]_i$ transients in RPA cell bodies *in vitro*. To consistently evoke action potentials, cells loaded with the Ca^{2+} indicator fura-2 AM were periodically depolarized by switching from normal saline (1.7 mM KCl) to saline containing an increased concentration of KCl (high-K⁺ saline). Because the excitability of individual cells differed, the KCl concentration of the high-K⁺ saline was adjusted to either 5, 10, or 20 mM to yield a robust but nonsaturating F_{340}/F_{380} response (i.e., mean $0.8 < F_{340}/F_{380} < 2$ in the periphery of the cell) (Fig. 2A,B). In each of the experiments, the cells were exposed to a sequence of high-K⁺ saline stimulations under peptide-free conditions before 1 μ M cGRGDSPA was added to the bath. Repeated stimulation of the cells with peptide-free high-K⁺ saline neither enhanced nor substantially fatigued the F_{340}/F_{380} response (Fig. 2). In the example shown, depolarization induced \sim 10 min after the introduction of 1 μ M cGRGDSPA in the bath resulted in a substantially enhanced response (Fig. 2A,B). Overall, the depolarization-induced F_{340}/F_{380} response was significantly potentiated after treatment with cGRGDSPA in 6 of the 14 cells tested (Fig. 2C). Although average resting F_{340}/F_{380} was not significantly altered in the presence of cGRGDSPA (ANOVA; $F_{(1,532)} = 0.466$; $p > 0.05$) in these six cells, we typically observed an increase in the frequency and amplitude of baseline fluctuation in the presence of the peptide (Fig. 2B). This effect may be associated with increased action-potential activity induced by the peptide, a hypothesis not formally tested.

To verify the specificity of the effects of RGD peptides on $[Ca^{2+}]_i$, we tested two other analogs, GRGDS and SDGRG. These peptides contain the same amino acids arranged in the opposite order. As a result, SDGRG, which lacks the essential RGD sequence, does not bind the FN receptor in RPA neurons (Wildering et al., 1998). High-K⁺ saline responses were induced sequentially in peptide-free medium after 20 min of exposure to 10 μ M SDGRG and after 20 min of exposure to 10 μ M GRGDS ($n = 6$). An example of the F_{340}/F_{380} intensity measured in one of

the horizontal bar; normalization: average pretreatment, $F_{340}/F_{380} = 1$, indicated by the horizontal dashed line in C). **C**, Average normalized F_{340}/F_{380} intensity measured in cells subjected to the experimental protocol outlined in B (mean \pm SEM; $n = 6$). Repeated depolarization of the cells before treatment with cGRGDSPA did not significantly affect the average F_{340}/F_{380} response. However, in the presence of cGRGDSPA (indicated by the horizontal bar and vertical dashed lines), the depolarization-induced F_{340}/F_{380} response was significantly enhanced ($p < 0.001$).

the cells tested is shown in Figure 3*A*. Again, repeated stimulation with peptide-free high- K^+ saline did not substantially alter the response. Moreover, a 20 min exposure to 10 μ M of the inactive analog SDGRG did not affect the high- K^+ saline response. In contrast, stimulation with high- K^+ saline after a 20 min exposure to 10 μ M SGRGD produced a markedly enhanced response. On average (Fig. 3*B*), the depolarization-evoked F_{340}/F_{380} response in the presence of SDGRG did not differ from the control response level (Tukey's HSD; $q = 1.005$; $p > 0.05$; $n = 6$), whereas in the presence of GRGDS, the response was significantly enhanced (Tukey's HSD; $q = 25.69$; $p < 0.001$; $n = 6$). Together, these results show that RGD peptides can substantially enhance depolarization-dependent $[Ca^{2+}]_i$ responses, and that this effect is a specific, receptor-mediated event.

The evidence presented thus far indicates that integrin ligands can induce rapid changes in electrical activity and depolarization-dependent $[Ca^{2+}]_i$ signaling in RPA neurons. However, these assays do not distinguish between indirect effects on $[Ca^{2+}]_i$ arising from an increase in action-potential frequency and/or changes in action-potential duration from direct effects resulting from modulation of Ca^{2+} influx through voltage-gated Ca^{2+} channels. Therefore, we tested the effects of RGD peptides on pharmacologically isolated HVA Ca^{2+} currents recorded from RPA neuron somata *in vitro*. RPA neurons express an HVA Ca^{2+} current that activates above a threshold of -40 mV and decays in a complex manner (Fig. 4*A*). We have shown previously that under conditions similar to the present ones, this current was completely inhibited by submillimolar doses of the inorganic Ca^{2+} -channel blocker $CdCl_2$ (Hermann et al., 1997). Although HVA Ca^{2+} currents in RPA neurons most closely resemble mammalian L-type Ca^{2+} currents, they are only partially inhibited by organic L-type Ca^{2+} -channel antagonists (W. C. Wildering, unpublished observation). Importantly, treatment with $CdCl_2$ did not reveal an underlying outward current, indicating that in our hands, the HVA Ca^{2+} current is not contaminated by a residual H^+ current as reported by Byerli and Suen (1989).

In these experiments, cells were routinely held at a membrane potential of -80 mV between test pulses and stepped to a test potential of 0 mV once every minute. This allowed us to monitor the stability of the current before peptide treatment as well as progression of the treatment effects. To include kinetically different parts of the current in the analysis, treatment effects were quantified by measuring the amplitude of the early peak (I_{peak}) and the late (I_{late}) current amplitudes measured after the rapidly decaying component had died out (i.e., 500 msec) (Fig. 4*A*). Experiments commenced once the kinetics of the current (I_{peak} and decay properties) had remained stable for at least 10 min after initiating whole-cell mode. Instantaneous current-voltage ($I-V$) relationships were sampled both immediately before peptide treatment and after the maximal treatment effect was attained.

We were able to satisfactorily record HVA Ca^{2+} currents for an extended period (>90 min after seal formation) from nine cells. Treatment with cGRGDSPA (1 μ M) caused a significant change in Ca^{2+} current in four of these nine cells. This effect typically developed over a matter of minutes but required several tens of minutes of continued exposure to the peptide to reach its peak (Fig. 5*B*). On average, I_{peak} increased from -2.16 ± 0.53 nA under control conditions to -3.31 ± 0.80 nA after treatment (mean \pm SEM; $n = 4$; measured at a test potential of $+10$ mV), an increase of 43% above control level. Comparison of the $I-V$ relationships acquired under both conditions reveals that al-

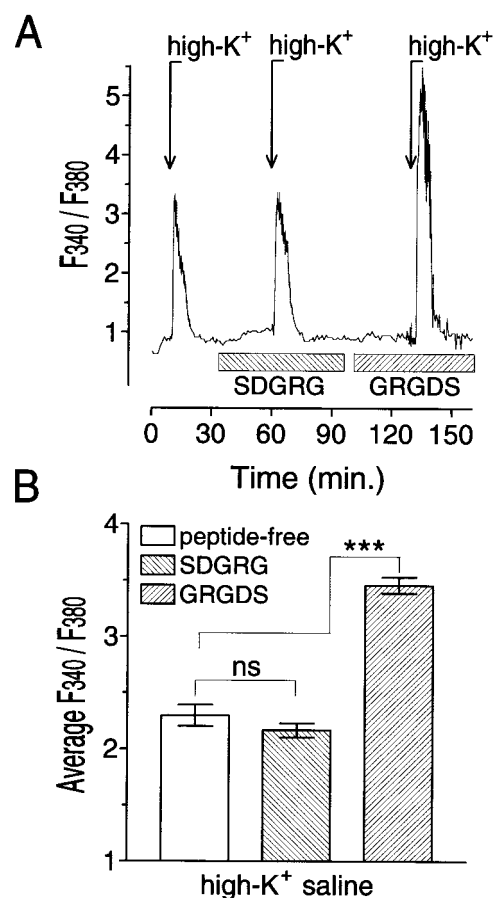


Figure 3. Sequence reversal abolished the ability of RGD peptides to enhance the depolarization-induced intracellular free Ca^{2+} response in isolated RPA neuron cell bodies. *A*, Normalized F_{340}/F_{380} signal measured in a region immediately inside the plasma membrane in an RPA cell body in normal saline and during depolarization with high-potassium saline (indicated by arrows marked high- K^+). After establishing a baseline and testing its high- K^+ response in peptide-free media, we exposed the cell in sequence to media containing a 10 μ M concentration of the inactive RGD peptide SDGRG and its active analog GRGDS (indicated by horizontal bars marked SDGRG and GRGDS, respectively). SDGRG did not substantially alter the depolarization-dependent F_{340}/F_{380} responses. GRGDS, conversely, significantly enhanced the response (data normalization; average pretreatment, $F_{340}/F_{380} = 1$). *B*, Mean F_{340}/F_{380} intensity measured in six cells during high-potassium saline-induced responses in peptide-free medium and in medium containing 10 μ M SDGRG or 10 μ M GRGDS; *** $p < 0.001$.

though peptide treatment had the largest absolute effect on the instantaneous current amplitude (i.e., I_{peak}), it enhanced the current over the entire duration of the 1 sec test pulse (Fig. 4*A–D*). This implies that integrin ligands can affect both transient and sustained components of the HVA Ca^{2+} current in RPA neurons.

In addition to cGRGDSPA, we tested other integrin ligands for their ability to modulate the HVA Ca^{2+} current. The following peptides induced a significant increase in current amplitude in a subset of the cells tested (mean current gain \pm SEM; I_{peak} measured at a test potential of $+10$ mV and normalized with respect to pretreatment control level): 1 μ g/ml FN, 1.750 ± 0.1800 (three of seven cells); 10 μ M RGD, 1.210 ± 0.0170 (four of nine cells); and 10 μ M GRGDS, 1.480 ± 0.0150 (three of seven cells). However, the inactive analog SDGRG did not significantly alter I_{peak} ($n = 5$).

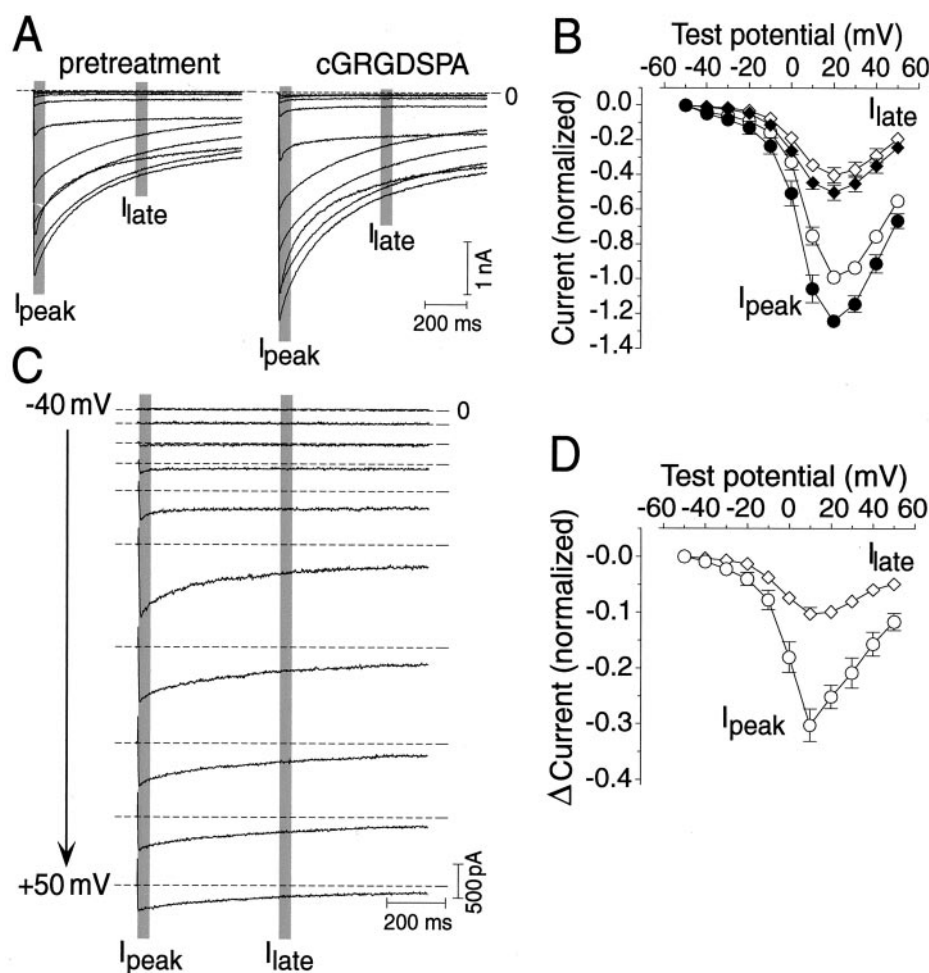


Figure 4. Integrin ligands enhance HVA Ca^{2+} currents in RPA neurons. *A*, Ca^{2+} current recorded in peptide-free medium (control) and after a 20 min treatment with 1 μM cGRGDSPA (cGRGDSPA). *B*, Average current-voltage relationship of I_{peak} (○ and ●) and I_{late} (◇ and ◇) obtained in peptide-free medium (○ and ◇) and after a 20 min treatment with 1 μM cGRGDSPA (● and ◇) (mean_{peak} = 1; holding potential of -80 mV; test potentials of -40 to +50 mV in increments of 10 mV). *C*, Differenced current (i.e., current in the presence of cGRGDSPA minus current before peptide treatment) at different test potentials ranging from -40 to +50 mV (in increments of 10 mV). Note that treatment with cGRGDSPA induced both rapidly and slowly decaying components of the current (horizontal dashed lines indicate zero current level). *D*, Average current-voltage relationship of the differenced I_{peak} (○) and I_{late} (◇) (mean_{peak} = 1). Both I_{peak} and I_{late} are enhanced over their entire voltage range, with a maximal current gain of ~30% of I_{peak} measured at a test potential of 10 mV.

In the experiments described above, we used near maximal doses as determined previously in a cell-adhesion assay (Wildering et al., 1998). Attempts to establish dose-response characteristics for the effects of cGRGDSPA on the HVA Ca^{2+} current revealed a peculiar divergence in the responsiveness of individual RPA neurons (Fig. 5). In these experiments, cells ($n = 14$) were sequentially exposed to a low (3 nM) and high (3 μM) concentration of cGRGDSPA. In some cells, we recorded a monotonic increase in current amplitude during exposure to different cGRGDSPA doses ($n = 4$) (Fig. 5*A,B*). Other cells responded in a biphasic manner ($n = 2$) (Fig. 5*C,D*). In those cases, the low concentration of cGRGDSPA induced a reduction in current amplitude, whereas the high concentration reversed this effect and caused the current to increase over the course of several tens of minutes to a final level exceeding the pretreatment control level (Fig. 5*C,D*).

DISCUSSION

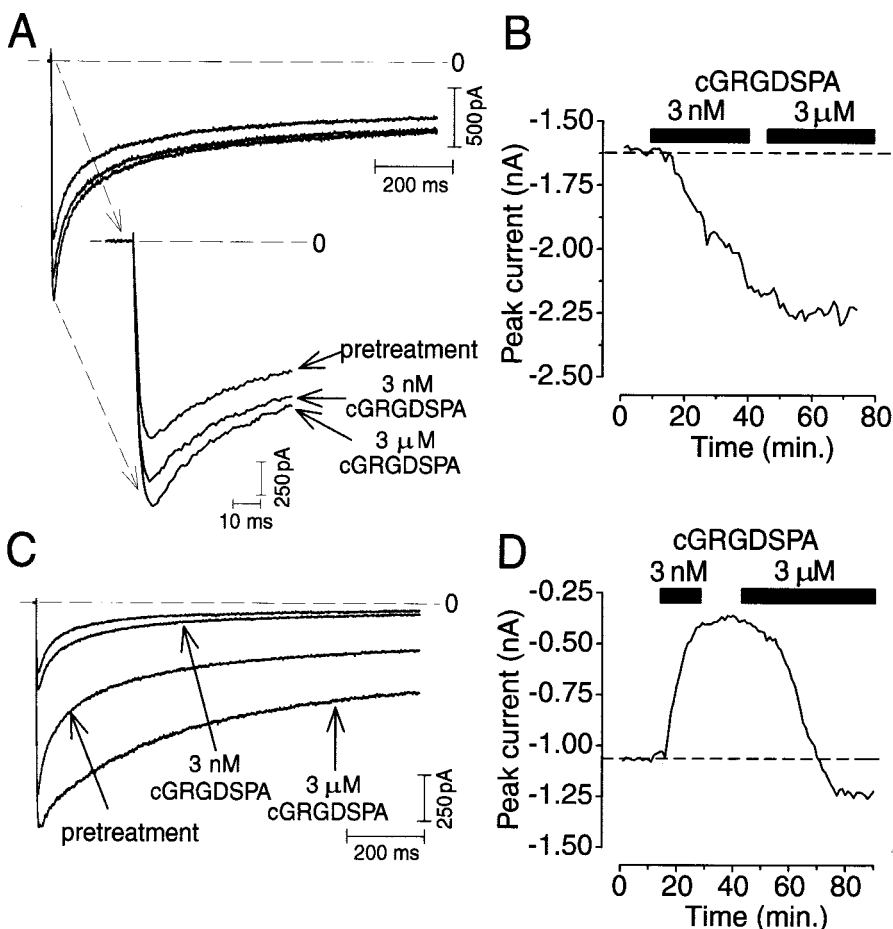
Our results demonstrate that soluble integrin ligands can induce changes in the electrophysiological properties of mature neurons in a matter of minutes, thus providing a novel perspective on the potential of integrins and their ligands as neuromodulators in the mature nervous system.

Our data suggest that integrin-associated signaling pathways target various channel types in the neuronal membrane. First of all, the results obtained in the fura-2 AM and whole-cell voltage-clamp assays clearly identify HVA Ca^{2+} channels as one of the

targets of these pathways in RPA neurons. We also show, however, that integrin ligands can trigger membrane depolarization and repetitive action-potential firing in previously quiescent RPA neurons *in vitro*. Although HVA Ca^{2+} channels may participate in the control of action-potential firing rates, it is unlikely, considering their high voltage-activation threshold (more than -40 mV), that they participate in the depolarization of the membrane from values less than -65 mV and the induction of action-potential firing activity. Thus, our results suggest that integrins also modulate subthreshold membrane channels involved in the control of neuronal excitability. Interestingly, the idea that other types of channels are also under the control of integrins is supported by a growing list of studies on a variety of non-neuronal cell types (for review, see Davis et al., 2001). In fact, there is evidence from studies on cell lines that integrins may interact with inward rectifier potassium channels (Arcangeli et al., 1993; McPhee et al., 1998). The outward currents carried by these channels probably participate in the control of resting membrane potential and repetitive firing.

Our finding that integrins modulate HVA Ca^{2+} currents in neurons is particularly significant, because such a link has been postulated (Bixby et al., 1994) but has never been formally tested. At present, our study provides the only direct electrophysiological evidence for integrin-dependent modulation of neuronal HVA Ca^{2+} channels. This raises the question of whether this effect is specific to *Lymnaea* neurons or whether our observations can be

Figure 5. Differential modulation of HVA Ca^{2+} currents by integrin ligands. **A**, HVA Ca^{2+} current recorded in sequence in peptide-free medium (trace denoted by pretreatment), after a 20 min exposure to 3 nM cGRGDSPA (trace denoted by 3 nM cGRGDSPA), and after a subsequent 20 min exposure to 3 μM cGRGDSPA (trace denoted by 3 μM cGRGDSPA); the inset shows the first 70 msec of the current record on a larger scale. Test pulse, +10 mV; holding potential, -80 mV (horizontal dashed line indicates zero current level). **B**, Time course of I_{peak} changes measured once per minute before treatment and in the presence of 3 nM and 3 μM cGRGDSPA (presence of the peptide at each of the doses is indicated by the two labeled horizontal bars; data correspond to data shown in **A**). Note that I_{peak} increased monotonically independent of the concentration of the peptide (horizontal dashed line indicates pretreatment control level). **C**, HVA Ca^{2+} current recorded in sequence in peptide-free medium (trace denoted by pretreatment), after a 20 min exposure to 3 nM cGRGDSPA (trace denoted by 3 nM cGRGDSPA), and after a subsequent 20 min exposure to 3 μM cGRGDSPA (trace denoted by 3 μM cGRGDSPA). Test pulse, +10 mV; holding potential, -80 mV (horizontal dashed line indicates zero current level). **D**, Time course of I_{peak} changes measured once per minute before treatment and in the presence of 3 nM and 3 μM cGRGDSPA (presence of the peptide at each of the doses is indicated by the two correspondingly labeled horizontal bars; data correspond to data shown in **C**). Note that in this case, I_{peak} decreased in response to the lower peptide concentration and increased only after the dose was raised to 3 μM (horizontal dashed line indicates pretreatment control level).



generalized. The notion that similar principles are at work in mammals, however, is supported by a study by Wu et al. (1998) on integrin-dependent modulation of L-type HVA Ca^{2+} currents in rat vascular smooth muscle. There are many striking parallels between our results and those of the aforementioned study. This similarity between two such phylogenetically diverse model systems suggests that integrin-dependent modulation of voltage-gated Ca^{2+} currents has an evolutionarily ancient origin and may be more common than previously thought.

Although our primary message is that integrins modulate neuronal HVA Ca^{2+} currents, several intriguing features are contained in the details of our results. First of all, we show that soluble integrin ligands can induce robust signaling responses in RPA neurons. This is an important observation, because the field of integrin signaling is dominated by the view that monovalent, soluble ligands have a limited capability of inducing signaling responses (Clark et al., 1994; Miyamoto et al., 1995). Our data add to a growing list of reports suggesting the contrary view (Rivas et al., 1992; Kuhn et al., 1998; Wu et al., 1998; Gomez et al., 2001).

Another intriguing feature of our results is the variability in responsiveness of individual cells, either reflected in a <100% responsiveness in any given assay (i.e., ~40% in each assay) or in the differential effects of different ligand concentrations on the HVA Ca^{2+} current. Incidentally, similar variability is found in the neurite outgrowth-inducing capacity of FN in RPA neurons *in vitro* (Wildering et al., 1998). Currently, we have no explanation for this phenomenon. There are reasons to believe, however, that differences in the integrin phenotype of individual cells may be at

play. Data from studies on various mammalian smooth and skeletal muscle types suggest that L-type Ca^{2+} channels are regulated by a variety of integrin heterodimers, with some coupled to facilitatory signaling pathways and others coupled to inhibitory signaling pathways (for review, see Davis et al., 2001). Particularly relevant in this context is the observation by Wu et al. (1998) that soluble ligands appear to preferentially activate certain integrin heterodimers. Thus, it is conceivable that variability in the responsiveness of RPA neurons to soluble ligands reflects differences in the integrin phenotype of individual cells, an avenue we need to explore further.

Alternative explanations are conceivable, however. For example, our previous studies (Wildering et al., 1995; Fainzilber et al., 1996) demonstrated that neurotrophic factor-signaling pathways participate in the regulation of HVA Ca^{2+} currents in RPA neurons. Hence, integrin and growth factor signaling pathways appear to converge at the level of the Ca^{2+} channels. It is therefore conceivable that these systems condition the signaling response of each other, an idea supported by a steadily growing body of literature (Plopper et al., 1995; Juliano, 1996; Grabham and Goldberg, 1997; Grabham et al., 2000).

Finally, the effects shown here generally had a long recovery time. It is unclear whether this is attributable to long-standing aftereffects of ligand binding on the signal transduction machinery of the integrin or to slow kinetics of the ligand-integrin dissociation process. Alternatively, it is not unthinkable that the integrin ligands (RGD peptides, FN) are not readily washed out of the environment of the cell and remain available for receptor binding. Additional studies need to be done to clarify this matter.

Recapitulating, our results provide firm evidence for a signaling link between neuronal voltage-gated Ca^{2+} channels and integrins. They also raise a number of intriguing questions with regard to the variability and adaptability of the integrin signaling system.

Our results are potentially relevant to diverse areas of neurobiology. For instance, seizure activity in the mammalian CNS has been associated with the regulation of ECM protein and integrin expression levels (Hoffman et al., 1998; Pinkstaff et al., 1998). Our finding that integrin ligands can induce a rapid increase in neuronal electrical activity suggests that elevated expression of these proteins may be a factor in the persistence of aberrant electrical activity that characterizes seizures.

Integrins and their ligands have also been implicated in the mechanism of learning and memory formation (for review, see Jones and Grooms, 1997; Murase and Schuman, 1999; Benson et al., 2000). Molecular genetic studies have uncovered a role for an integrin homolog in the acquisition of olfactory memory in fruit flies (Grotewiel et al., 1998). Also, RGD peptides have been shown to interfere with consolidation of long-term potentiation in the mammalian hippocampus (Stäubli et al., 1998). Considering that modulation of Ca^{2+} influx is one of the initiating factors in most forms of synaptic plasticity, our results suggest that integrin-mediated modulation of voltage-gated Ca^{2+} currents may be one of the factors involved.

A third area of interest is that of ECM-dependent control of neurite outgrowth during development and regeneration. Numerous studies implicate ECM proteins, $[\text{Ca}^{2+}]_i$, and Ca^{2+} influx in the control of neurite outgrowth and target finding (Kater and Mills, 1991; Rivas et al., 1992; Letourneau et al., 1994a,b; McKerracher et al., 1996; Kuhn et al., 1998; Zheng, 2000; Gomez et al., 2001). Tentatively, the capacity of the integrin to differentially modulate voltage-gated Ca^{2+} currents may be involved in the ability of navigating cells and neurites to detect gradients of ECM proteins or to engage in substratum selection, a process uniquely sensitive to small changes in Ca^{2+} influx and $[\text{Ca}^{2+}]_i$. Our present understanding of the role of integrin-mediated modulation of voltage-gated Ca^{2+} channels in these processes is, however, not without contradictions. In particular, although Bixby et al. (1994) suggested that these channels are instrumental in the trophic effects of ECM proteins, most recent studies emphasize a role for voltage-independent Ca^{2+} -influx pathways (Kuhn et al., 1998; Gomez et al., 2001). In this context, it is important to recognize that both our work and that of Bixby et al. (1994) differ from most other studies in that integrin ligands are applied to the entire cell rather than to parts of the cell such as the growth cone. This suggests that regional differences in integrin signaling and/or coupling of integrins to Ca^{2+} channels may exist within neurons.

In summary, we provide evidence that integrins are capable of relatively rapid neuromodulatory actions in mature neurons, a hitherto largely unexplored aspect of integrin–ECM physiology. Our data show that voltage-gated Ca^{2+} channels are one of the targets of integrin signaling pathways and suggest that other (subthreshold) currents may also be modulated by these pathways. Moreover, the results suggest that integrin-associated signaling pathways possess considerable flexibility in the control of excitable properties of the neural membrane. Thus, our results warrant a further exploration of these mechanisms and their relevance in the physiology of the mature nervous system.

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